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นางสาว ณัฐชนัญ ศิโรรัตน์สกุล

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DEVELOPMENT OF OSMOTICALLY CONTROLLED DRUG DELIVERY CAPSULES

Miss Natchanan Siroratsakul

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การพัฒนาระบบออสโมติกของแคปซูลเจละตินชนิดแข็งเคลือบด้วยฟิล์มชนิดกึ่งซึมผ่าน เคลือบแคปซูลเจลาตินด้วยเครื่องเคลือบฟลูอิดไคซ์เบคโคยมีไฮครอกซีโพรพิลเมทธิล ได้ เซลลูโลสเป็นชั้นรองและเซลลูโลสอะซีเตตเป็นสารก่อฟิล์มชนิคกึ่งซึมผ่านได้ ใช้โพรพราโนลอล ไฮโครคลอไรค์เป็นยาต้นแบบ ใช้โซเคียมคลอไรค์ โปแตสเซียมคลอไรค์ แลคโตส และซูโครส เป็นสารก่อออสโมติก ทำการศึกษาปัจจัยที่มีอิทธิพลต่อการปลดปล่อยยา เช่น ขนาครู ปริมาณ พลาสติไซเซอร์ ปริมาณสารก่อแรงดันออสโมติก ความแรงของแรงดันออสโมติกในสารละลายที่ ใช้ทดสอบการปลดปล่อยยา ในการเคลือบใช้พี่อีจี400เป็นพลาสติไซเซอร์และสารก่อเกิดร ภาพถ่ายจากกล้องจุลทรรศน์อิเล็กตรอนแสดงให้เห็นว่ามีการสร้างรูขึ้นภายในฟิล์มเซลลูโลสอะซึ เตตหลังจากที่แคปซูลที่ถูกเคลือบนั้นได้สัมผัสน้ำ การปลดปล่อยยาจะเพิ่มมากขึ้นเมื่อปริมาณของ พีอีจี400เพิ่มมากขึ้นโดยที่พีอีจี400สามารถละลายออกจากฟิล์มเซลลูโลสอะซีเตตเนื่องด้วย คุณสมบัติความชอบน้ำของพี่อีจี<mark>400ขนาดรูมีอิทธิพลอย่างมากต่อการปลดปล่อยยาเมื่อ</mark>ฟิล์มมีขนาด ในทางตรงกันข้า<mark>มขนาดรูมีอิทธิพล</mark>เพียงเล็กน้อยต่อการปลดปล่อยยาเมื่อฟิล์มมี การปลดปล่อยยาเพิ่มมากขึ้นเมื่อปริมาณ โซเดียมคลอไรค์ในตำรับเพิ่มมากขึ้น ยกเว้นตำรับที่ประกอบด้วยแลคโตสอย่างเดียวที่มีการปลดปล่อยยามากที่สุด โซเดียมคลอไรด์ใน **ตำร**ับอาจจะเหนี่ยวนำให้เกิดการเกาะตัวกันของเจลาตินอันเนื่องมาจากปฏิกิริยาระหว่างเจลาติน และโซเคียมคลอไรค์เป็นผลให้เกิดการขวางทางน้ำที่เข้าระบบคังนั้นการปลดปล่อยยาจึงลดลง แต่ ทว่าแลก โตสนั้น ไม่เหนี่ยวนำให้เกิดการเกาะตัวกันของเจลาตินซึ่งทำให้การปลดปล่อยยามากกว่า เมื่อแรงคันออสโมติกของสารละลายที่ใช้ในการทคสอบการปลคปล่อยยาเพิ่มมากขึ้นการ ปลดปล่อยยาจะลดลง ความแตกต่างของแรงดันออสโมติกภายในและภายนอกระบบลดลงอาจเป็น สาเหตุหนึ่งในการปลดปล่อยยาลดลง

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KEY WORD: OSMOTIC PUMP / CAPSULE / FILM COATING / FLUIDIZED

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NATCHANAN SIRORATSAKUL: THESIS TITLE. DEVELOPMENT OF OSMOTICALLY CONTROLLED DRUG DELIVERY CAPSULES THESIS ADVISOR: ASSOC. PROF. POJ KULVANICH, Ph.D., 247 pp. ISBN

Osmotic system of coated hard gelatin capsule was developed. Gelatin capsule shell was coated by fluidized bed coater using hydroxypropylmethylcellulose and cellulose acetate as subcoating layer and semipermeable membrane, respectively. Propranolol hydrochloride was used as a model drug. NaCl, KCl, lactose and sucrose were used as osmotic agents. Various influential factors ie. orifice size, amount of plasticizer, amount of osmotic agent, osmotically active dissolution medium were investigated. PEG400 was used as plasticizer and pore forming agent. SEM photomicrograph shows porous cellulose acetate membrane after coated capsule contacted the water. The drug release increased as amount of PEG400 was increased as PEG400 could leach out from the cellulose acetate film due to hydrophilic property causing porous structure of the membrane. At the low thickness of coating membrane, the orifice size influenced dramatically on drug release. On the contrary, the orifice size influenced slightly on drug release at the high thickness of coating membrane. The drug release rate increased when amount of sodium chloride in formulation was increased. Whereas, the drug release rate of formulation containing lactose was the highest. Sodium chloride in the formulation might induce aggregation of dissolved gelatin shell due to interaction between gelatin and sodium chloride resulting in obstructing water influx into the coated capsule hence less drug release. Whereas, lactose did not induce aggregation of dissolved gelatin shell resulting in higher drug release. When osmotic pressure of dissolution medium was increased, the drug release decreased. Decreased osmotic pressure difference across the membrane might be a cause of slower drug release rate.

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LIST OF ABBREVIATIONS

ANOVA analysis of variance

CA cellulose acetate

CV coefficient of variation

i.e. example and other

et all et alli and other

g. gram(s)
hr. hour(s)

HCl hydrochloric acid or hydrochloride

ml. milliliter (s)

R² coefficient of determination

SD standard deviation

SEM scanning electron photomicrograph

UV ultraviolet

w/w weight by weight

μm micrometer(s)

% percentage

DEP diethyl phthalate

PEG 400 polyethylene glycol 400

HPMC hydroxypropylmethylcellulose

PG propylene glycol

nm. nanometre μg. microgram

M molarity (mole/litre)

RDT relative dissolution time

AUC area under dissolution curve

CV coefficient variation

mm. millimetre

rpm. round per minute

mosm. milliosmolarity