

REFERENCE

- Ayhan, H. and Ayhan, F. (2002) In Vitro Evaluation of 3T3 and MDBK Cells Attachment and Proliferation on Collagen and Fibronectin Immobilized Nonwoven Polylactide Matrices. Journal of Bioactive and Compatible Polymers. 17, 463-476.
- Boelgen, N., Menciloglu, Y.Z., Acatay, K., Vargel, I., and Piskin, E. (2005) In vitro and in vivo degradation of non-woven materials made of poly(ϵ -caprolactone) nanofibers prepared by electrospinning under different conditions. Journal of Biomaterials Science. Polymer Edition, 16(12), 1537-1555.
- Burg, K.J.L., Porter, S., and Kellam, J.F. (2000) Biomaterial developments for bone tissue engineering. Biomaterials, 21, 2347-2359.
- Calvert, J.W., Marra, K.G., Cook, L., Kumta, P.N., DiMilla, P.A., and Weiss, L.E. (2000) Characterization of osteoblast-like behavior of cultured bone marrow stromal cells on various polymer surfaces. Journal of Biomedical Materials Research, 52(2), 279-284.
- Carter, D. C. and Ho, J. X. (1994) Structure of Serum Albumin. Advance in Protein Chemistry. 45, 153-203.
- Cheng, Z., and Teoh, S.-H. (2004) Surface modification of ultra thin poly(ϵ -caprolactone) films using acrylic acid and collagen. Biomaterials, 25(11), 1991-2001.
- Edlund, U., Dänmark, S., and Albertsson, A.-C. (2008) A Strategy for the Covalent Functionalization of Resorbable Polymers with Heparin and Osteoinductive Growth Factor. Biomacromolecules, 9(3), 901-905.
- Figge, J., Rossing, T. H. and Fencl, V. (1991) The Role of serum-proteins in Acid-Base Equilibria. The Journal of Laboratory and Clinical Medicine. 117, 453 - 467.
- Gao, C., Guan, J., Zhu, Y., and Shen, J. (2003) Surface Immobilization of Bioactive Molecules on Polyurethane for Promotion of Cytocompatibility to Human Endothelial Cells. Macromolecular Bioscience, 3(3-4), 157-162.

- Guan, J., Gao, C., Feng L., and Shen, J. (2001) Surface modification of polyurethane for promotion of cell adhesion and growth 1: Surface photo-grafting with N,N-dimethylaminoethyl methacrylate and cytocompatibility of the modified surface. Journal of Materials Science: Materials in Medicine., 12 (5), 447-452
- Habraken, W.J.E.M., Wolke, J.G.C., and Jansen, J.A. (2007) Ceramic composites as matrices and scaffolds for drug delivery in Tissue engineering. Advanced drug delivery review, 59, 234-248.
- Hou, Q., Grijpma, D. W., Feijen, J. (2003) Porous polymeric structures for tissue engineering prepared by a coagulation, compression moulding and salt leaching technique. Biomaterials 24(11), 1937-1947.
- Huang, W., Carlsen, B., Wulur, I., Rudkin, G., Ishida, K., Wu, B., Yamaguchi, D.T., Miller, T.A. (2004) BMP-2 exerts differential effects on differentiation of rabbit bone marrow stromal cells grown in two-dimensional and three-dimensional systems and is required for in vitro bone formation in a PLGA scaffold. Experimental Cell Research , 299, 325– 334
- Hutmacher, D. W. (2000) Scaffolds in tissue engineering bone and cartilage. Biomaterials, 21, 2259.
- Jeon, O., Song, S.J., Kanga, S-W., Putnam, A.J., and Kim, B-S. (2007) Enhancement of ectopic bone formation by bone morphogenetic protein-2 released from a heparin-conjugated poly(L-lactic-co-glycolic acid) scaffold Biomaterials; 28: 2763–2771
- Lee, S-H., and Shin, H. (2007) Matrices and scaffolds for delivery of bioactive molecules in bone and cartilage tissue engineering. Advanced drug delivery reviews ,59, 339-359.
- LeGero, R.Z. (2002) Properties of osteoconductive biomaterials: calcium phosphates. Clin Orthop Relat Res, 395, 81-98.
- Ma, Z., Gao, C., Yuan, J., Ji, J., Gong, Y., and Shen, J. (2002) Surface modification of poly-L-lactide by photografting of hydrophilic polymers towards improving its hydrophilicity. Journal of Applied Polymer Science, 85 (10), 2163 – 2171

- Mattanavee, W., Suwantong, O., Puthong, S., Bunaprasert, T., Hoven, V.P., and Supaphol, P. (2009) Immobilization of Biomolecules on the Surface of Electrospun Polycaprolactone Fibrous Scaffolds for Tissue Engineering. ACS Applied Materials & Interfaces.
- Meinel, L., Zoidis, E., Zapf, J., Hassa, P., Hottiger, M.O., Auer, J.A., Schneider, R., Gander, B., Luginbuehl, V., Wolfisberger, R.B., Illi, O.E., Merkle, H.P., and Rechenberg, B. von. (2003) Localized insulin-like growth factor I delivery to enhance new bone formation. *Bone*; 33 : 660–672
- Mikos, A.G., Bao, Y., Cima, L.G., Ingber, D.E., Vacanti, J.P., Langer, R. (1993) Preparation of poly (glycolic acid) bonded fibres structures for cell attachment and transplantation. Journal of biomedical materials research, 27, 183-189.
- Mikos, A.G., Sarakinos, G., Vacanti, J.P., Langer, R., and Cima, L.G. (1996) Biocompatible polymer membranes and methods of preparation of three dimensional membrane structures. United States Patent 5514378
- Mikos, A.G., Thorsen, A.J., Czerwonka, L.A., Bao, Y., Langer, R. (1994) Preparation and characterisation of poly(L-lactic acid) foams. Polymer, 35, 1068-1077.
- Park, K., Jung, H.J., Kim, J.-J., Ahn, K.-D. and Han, D.K. (2006) Acrylic Acid-Grafted Hydrophilic Electrospun Nanofibrous Poly(L-lactic acid) Scaffold. Macromolecular Research, 14 (5), 552-558
- Prasansuklarb, A. (2008) Osteoblastic cell growth and enzymatic degradation of different aliphatic polyester scaffolds. Master thesis. The Petroleum and Petrochemical College, Chulalongkorn University.
- Saito, N., Okada, T., Horiuchi, H., Ota, H., Takahashi, J., Murakami, N., Nawata, M., Kojima, S., Nozaki, K., and Takaoka, K. (2003) Local bone formation by injection of recombinant human bone morphogenetic protein-2 contained in polymer carriers. *Bone*, 32, 381–386
- Salgado, A.J., Coutinho, O.P., and Reis, R.L. (2004) Bone Tissue Engineering: State of the Art and Future Trends. Macromolecular Bioscience; 4 : 743–765

- Santiago, L.Y., Nowak, R.W., Rubin, J.P., and Marra, K.G. (2006) Peptide-surface modification of poly(caprolactone) with laminin-derived sequences for adipose-derived stem cell applications. *Biomaterials*, 27(15), 2962-2969.
- Savarino, L., Baldini, N., Greco, M., Capitani, O., Pinna, S., Valentini, S., Lombardo, B., Esposito, M.T., Pastore, L., Ambrosio, L., Battista, S., Causa, F., Zeppetelli, S., Guarino, V., and Netti, P.A. (2007) The performance of poly- ϵ -caprolactone scaffolds in a rabbit femur model with and without autologous stromal cells and BMP4. *Biomaterials*, 28(20), 3101-3109.
- Shen, H., Hu, X., Yang, F., Bei, J., and Wang, S. (2009) The bioactivity of rhBMP-2 immobilized poly(lactide-co-glycolide) scaffolds. *Biomaterials*, 30(18), 3150-3157.
- Sumner, D.R., Turner, T.M., Urban, R.M., Leven, R.M., Hawkins, M., Nichols, E.H., McPherson, J.M., and Galante, J.O. (2001) Locally delivered rhTGF- β_2 enhances bone ingrowth and bone regeneration at local and remote sites of skeletal injury. *Journal of Orthopaedic Research*, 19, 85-94.
- Venugopal, J.R., Low, S., Choon, A.T., Kumar, A.B., and Ramakrishna, S. (2008) Nanobioengineered Electrospun Composite Nanofibers and Osteoblasts for Bone Regeneration. *Artificial Organs*, 32(5), 388-397.
- Wang, X., Wenk, E., Zhang, X., Meinel, L., Vunjak-Novakovic, G., and Kaplan, D.L. (2009) Growth factor gradients via microsphere delivery in biopolymer scaffolds for osteochondral tissue engineering. *Journal of Controlled Release*, 134, 81-90.
- Ward, A.G.; Courts, A. (1977) *The Science and Technology of Gelatin*. New York: Academic Press
- Wei, G., Jin, O., Giannobile, W.V., and Ma, P.X. (2007) The enhancement of osteogenesis by nano-fibrous scaffolds incorporating rhBMP-7 nanospheres. *Biomaterials*, 28, 2087-2096
- Wenk, E., Meinel, A.J., Wildy, S., Merkle, H.P., and Meinel, L. (2009) Microporous silk fibroin scaffolds embedding PLGA microparticles for controlled growth factor delivery in tissue engineering. *Biomaterials*, 30, 2571-2581

- Whang, K., Thomas, C. H., Healy, K. E. and Nuber, G. (1995) A novel method to fabricate bioabsorbable scaffolds. Polymer, 36, 837-842
- Woo, B.H., Fink, B.F., Page, R., Schrier, J.A., Jo, Y.W., Jiang, G., DeLuca, M., Vasconez, H.C., and DeLuca, P.P. (2001) Enhancement of Bone Growth by Sustained Delivery of Recombinant Human Bone Morphogenetic Protein-2 in a Polymeric Matrix. Pharmaceutical Research, 18(12)
- Yoneda, M., Teraia, H., Imaia, Y., Okada, T., Nozaki, K., Hikaruino, Miyamoto, S., and Takaoka, K. (2005) Repair of an intercalated long bone defect with a Synthetic biodegradable bone-inducing implant. Biomaterials, 26, 5145-5152
- Yoshimoto, H., Shin, Y.M., Terai, H., and Vacanti, J.P. (2003) A biodegradable nanofiber scaffold by electrospinning and its potential for bone tissue engineering. Biomaterials, 24(12), 2077-2082.
- Zhu, Y., Chian, K.S., Chan-Park, M.B., Mhaisalkar, P.S., and Ratner, B.D. (2006) Protein bonding on biodegradable poly(l-lactide-co-caprolactone) membrane for esophageal tissue engineering. Biomaterials, 27(1), 68-78.
- Zhu, Y., Cao, Liu, Y., and Shen, J. (2004) Endothelial cell functions in vitro cultured on poly(L-lactic acid) membranes modified with different methods. Journal of Biomedical Materials Research Part A, 69A(3), 436-443.
- Zhu, Y., Gao, C., Liu, X., and Shen, J. (2002a) Surface Modification of Polycaprolactone Membrane via Aminolysis and Biomacromolecule Immobilization for Promoting Cytocompatibility of Human Endothelial Cells. Biomacromolecules, 3(6), 1312-1319.
- Zhu, Y., Gao, C., and Shen, J. (2002 b) Surface modification of polycaprolactone with poly(methacrylic acid) and gelatin covalent immobilization for promoting its cytocompatibility. Biomaterials, 23(24), 4889-4895.

APPENDICES

Appendix A Experimental Data of Density, Porosity and Pore Volume

The density of the scaffolds ($\rho_{\text{scaffolds}}$) can be calculated using the following equation

$$\text{Apparent density } (\rho_{\text{scaffolds}} \text{ g/cm}^3) = \frac{m}{t \times A}$$

where m is the mass of the scaffold (g), t is the thickness of the scaffold (cm) and A is the area of the scaffold (cm²)

The porosity and pore volume of the scaffolds can be calculated using the following equation (Hou *et al.* 2003)

$$\text{Porosity (\%)} = \left(1 - \frac{\rho_{\text{scaffold}}}{\rho_{\text{polymer}}} \right) \times 100$$

$$\text{Pore volume} = \left(\frac{1}{\rho_{\text{scaffold}}} - \frac{1}{\rho_{\text{polymer}}} \right)$$

where ρ_{scaffold} is the apparent density of the fibrous scaffolds (g/cm³) and ρ_{polymer} is the density of the non-fibrous polymer (ρ_{polymer} of PCL is 1.145 g/cm³).

Table A1 Raw data of the density, porosity and pore volume of the unmodified PCL scaffolds and modified PCL scaffolds

| Material | weight(g) | thickness(mm) | | | | | density ($\times 10^{-2}$ g/cm ³) | porosity (%) | pore volume (cm ³ /g) |
|---------------------------|-----------|---------------|-------|-------|-------|-------|---|--------------|-------------------------------------|
| | | 1 | 2 | 3 | avg | SD | | | |
| Neat PCL (control) | 0.006 | 0.077 | 0.073 | 0.080 | 0.077 | 0.004 | 5.00 | 95.63 | 19.13 |
| | 0.004 | 0.075 | 0.056 | 0.056 | 0.062 | 0.011 | 4.27 | 96.27 | 22.53 |
| | 0.004 | 0.052 | 0.052 | 0.046 | 0.050 | 0.003 | 4.94 | 95.69 | 19.38 |
| | 0.007 | 0.110 | 0.116 | 0.121 | 0.116 | 0.006 | 4.16 | 96.37 | 23.19 |
| | 0.004 | 0.056 | 0.045 | 0.049 | 0.050 | 0.006 | 5.07 | 95.57 | 18.86 |
| Aminolyzed PCL | 0.005 | 0.054 | 0.063 | 0.051 | 0.056 | 0.006 | 5.22 | 95.44 | 18.28 |
| | 0.006 | 0.072 | 0.071 | 0.072 | 0.072 | 0.001 | 5.36 | 95.32 | 17.78 |
| | 0.007 | 0.121 | 0.107 | 0.116 | 0.115 | 0.007 | 3.80 | 96.68 | 25.47 |
| | 0.006 | 0.118 | 0.119 | 0.110 | 0.116 | 0.005 | 3.54 | 96.91 | 27.39 |
| | 0.007 | 0.121 | 0.127 | 0.139 | 0.129 | 0.009 | 3.32 | 97.10 | 29.21 |
| Activated PCL | 0.009 | 0.148 | 0.148 | 0.148 | 0.148 | 0.000 | 3.91 | 96.59 | 24.73 |
| | 0.009 | 0.160 | 0.140 | 0.150 | 0.150 | 0.010 | 3.98 | 96.52 | 24.23 |
| | 0.007 | 0.108 | 0.100 | 0.104 | 0.104 | 0.004 | 4.12 | 96.40 | 23.38 |
| | 0.008 | 0.163 | 0.139 | 0.151 | 0.151 | 0.012 | 3.57 | 96.88 | 27.13 |
| | 0.009 | 0.177 | 0.158 | 0.017 | 0.117 | 0.088 | 5.10 | 95.55 | 18.75 |
| gelatin A immobilized PCL | 0.007 | 0.144 | 0.148 | 0.139 | 0.144 | 0.005 | 2.94 | 97.43 | 33.15 |
| | 0.005 | 0.077 | 0.080 | 0.077 | 0.078 | 0.002 | 4.41 | 96.14 | 21.78 |
| | 0.007 | 0.134 | 0.132 | 0.119 | 0.128 | 0.008 | 3.49 | 96.95 | 27.76 |
| | 0.008 | 0.178 | 0.178 | 0.018 | 0.125 | 0.092 | 4.22 | 96.31 | 22.81 |
| | 0.005 | 0.052 | 0.036 | 0.149 | 0.079 | 0.061 | 3.70 | 96.77 | 26.15 |
| gelatin B immobilized PCL | 0.007 | 0.133 | 0.143 | 0.014 | 0.097 | 0.072 | 4.98 | 95.65 | 19.22 |
| | 0.008 | 0.173 | 0.171 | 0.176 | 0.173 | 0.003 | 2.85 | 97.51 | 34.24 |
| | 0.007 | 0.136 | 0.149 | 0.121 | 0.135 | 0.014 | 3.12 | 97.28 | 31.18 |
| | 0.009 | 0.199 | 0.185 | 0.187 | 0.190 | 0.008 | 3.07 | 97.32 | 31.68 |
| | 0.006 | 0.110 | 0.102 | 0.094 | 0.102 | 0.008 | 3.95 | 96.55 | 24.45 |
| BSA immobilized PCL | 0.008 | 0.143 | 0.145 | 0.014 | 0.101 | 0.075 | 4.90 | 95.72 | 19.54 |
| | 0.003 | 0.055 | 0.047 | 0.044 | 0.049 | 0.006 | 3.60 | 96.85 | 26.87 |
| | 0.007 | 0.149 | 0.158 | 0.145 | 0.151 | 0.007 | 3.02 | 97.36 | 32.26 |
| | 0.007 | 0.132 | 0.143 | 0.139 | 0.138 | 0.006 | 3.44 | 97.00 | 28.23 |
| | 0.005 | 0.097 | 0.054 | 0.086 | 0.079 | 0.022 | 4.28 | 96.27 | 22.51 |
| CBP immobilized PCL | 0.0044 | 0.053 | 0.064 | 0.049 | 0.055 | 0.008 | 5.17 | 95.49 | 18.49 |
| | 0.0072 | 0.141 | 0.12 | 0.128 | 0.130 | 0.011 | 3.61 | 96.85 | 26.85 |
| | 0.0049 | 0.072 | 0.084 | 0.085 | 0.080 | 0.007 | 3.96 | 96.54 | 24.36 |
| | 0.0029 | 0.037 | 0.028 | 0.031 | 0.032 | 0.005 | 5.89 | 94.86 | 16.11 |
| | 0.0056 | 0.082 | 0.087 | 0.085 | 0.085 | 0.003 | 4.30 | 96.25 | 22.40 |

APPENDICES

Appendix B Experimental Data of Water Retention Capacity and Weight Loss of Polycaprolactone Electrospun Fibrous Scaffolds

1. Water Retention Capacity

The water retention was calculated by using the following equation. (Kothapalli *et al.*, 2005)

$$\text{Water Retention (\%)} = \left(\frac{M_{wet} - M_{dry}}{M_{dry}} \right) \times 100$$

where M_{dry} and M_{wet} are the weight of the scaffold before and after immersion in 0.1 M PBS solution respectively. Five measurements were performed for the calculation of an average water retention value.

2. Degradation Study of Fibrous Scaffolds

The rate of degradation can be calculated using the following equation.

$$\text{Weight loss (\%)} = \left(\frac{M_f - M_i}{M_i} \right) \times 100$$

where M_i is the initial weight of the scaffolds and M_f and is the weight of the scaffold at the given degradation time point, immersed in 0.1 M PBS solution. Five measurements were performed for the calculation of an average water degradation rate value.

Table B1 Raw data of water retention capacity of aminolyzed PCL electrospun fibrous scaffolds at various HMD treatments

| Time(h) | water retention (%) | | | | | | | | | | | | | | | | | | | |
|---------------------------|---------------------|------|--------|------|--------|------|--------|------|--------|------|--------|------|--------|------|--------|------|--------|------|--------|------|
| | 0.25 | | 0.5 | | 1 | | 2 | | 4 | | 6 | | 12 | | 18 | | 24 | | 48 | |
| Sample | avg | SD | avg | SD | avg | SD | avg | SD | avg | SD | Avg | SD | avg | SD | avg | SD | avg | SD | avg | SD |
| Neat PCL | 56.93 | 0.4 | 61.31 | 0.16 | 66.64 | 0.26 | 82.66 | 1.11 | 119.56 | 0.69 | 125.96 | 0.34 | 133.14 | 0.76 | 136.99 | 0.94 | 140.00 | 0.45 | 140.50 | 0.28 |
| 0.04 g/ml HMD treated PCL | 81.36 | 0.59 | - | - | 89.44 | 0.57 | 97.10 | 0.62 | 153.00 | 0.49 | 182.00 | 0.75 | - | - | 200.00 | 0.66 | - | - | 212.29 | 1.39 |
| 0.06 g/ml HMD treated PCL | 93.29 | 1.41 | - | - | 95.27 | 1.74 | 101.46 | 0.93 | 204.13 | 0.62 | 225.18 | 1.42 | - | - | 236.16 | 1.23 | - | - | 263.38 | 1.44 |
| 0.08 g/ml HMD treated PCL | 183.49 | 0.91 | - | - | 217.04 | 0.91 | 231.98 | 0.55 | 234.71 | 0.3 | 235.35 | 1.42 | - | - | 255.51 | 0.83 | - | - | 273.04 | 0.49 |
| 0.10 g/ml HMD treated PCL | 200.00 | 0.61 | - | - | 228.13 | 0.41 | 235.60 | 0.35 | 245.98 | 1.23 | 254.69 | 1.27 | - | - | 273.09 | 1.06 | - | - | 278.39 | 0.7 |
| 0.20 g/ml HMD treated PCL | 228.45 | 0.9 | - | - | 235.57 | 0.76 | 244.80 | 1.4 | 247.53 | 0.98 | 259.86 | 0.76 | - | - | 277.39 | 0.95 | - | - | 289.74 | 0.93 |
| 0.40 g/ml HMD treated PCL | 196.26 | 0.47 | 213.24 | 0.7 | 225.87 | 0.77 | 242.60 | 0.31 | 254.61 | 0.17 | 257.69 | 0.53 | 261.33 | 0.81 | 271.98 | 0.25 | 280.00 | 0.78 | 300.42 | 1.3 |

Table B2 Raw data of water retention capacity of aminolyzed PCL electrospun fibrous scaffolds at various HMD treatments

| Time(h) | weight loss (%) | | | | | | | | | | | | | | | | | | | |
|---------------------------|-----------------|------|------|------|------|------|------|------|------|------|------|------|------|------|------|------|------|------|------|------|
| | 0.25 | | 0.5 | | 1 | | 2 | | 4 | | 6 | | 12 | | 18 | | 24 | | 48 | |
| Sample | avg | SD | avg | SD | avg | SD | avg | SD | avg | SD | Avg | SD | avg | SD | avg | SD | avg | SD | avg | SD |
| Neat PCL | 0.00 | 0.35 | 0.30 | 0.45 | 1.06 | 0.12 | 1.08 | 0.09 | 1.20 | 0.14 | 1.80 | 0.15 | 3.18 | 0.05 | 3.23 | 0.38 | 4.42 | 0.40 | 4.47 | 0.15 |
| 0.04 g/ml HMD treated PCL | 1.89 | 0.13 | - | - | 2.62 | 0.13 | 2.63 | 0.23 | 2.75 | 0.24 | 2.94 | 0.19 | - | - | 3.03 | 0.22 | - | - | 3.99 | 0.33 |
| 0.06 g/ml HMD treated PCL | 0.48 | 0.46 | - | - | 0.74 | 0.47 | 0.96 | 0.27 | 1.17 | 0.18 | 1.41 | 0.43 | - | - | 1.79 | 0.32 | - | - | 3.04 | 0.34 |
| 0.08 g/ml HMD treated PCL | 0.55 | 0.79 | - | - | 1.43 | 0.81 | 1.51 | 0.48 | 1.79 | 0.30 | 2.73 | 0.89 | - | - | 3.45 | 0.59 | - | - | 4.84 | 0.33 |
| 0.10 g/ml HMD treated PCL | 0.00 | 0.49 | - | - | 0.74 | 0.31 | 1.23 | 0.25 | 2.13 | 0.41 | 3.58 | 0.57 | - | - | 3.61 | 0.29 | - | - | 3.68 | 0.28 |
| 0.20 g/ml HMD treated PCL | 1.14 | 0.47 | - | - | 2.50 | 0.25 | 3.03 | 0.40 | 3.71 | 0.31 | 4.26 | 0.15 | - | - | 4.76 | 0.23 | - | - | 5.56 | 0.29 |
| 0.40 g/ml HMD treated PCL | 0.49 | 0.16 | 0.68 | 0.07 | 0.68 | 0.21 | 0.93 | 0.07 | 2.72 | 0.06 | 3.64 | 0.14 | 4.47 | 0.11 | 5.24 | 0.05 | 6.80 | 0.21 | 7.09 | 0.42 |

APPENDICES

Appendix C Experimental Data of NH_2 Density, Elemental Composition of the Surface and Water Contact Angle Measurement

1. NH_2 Density on the Modified PCL Scaffold

The ninhydrin analysis method was carried out to quantitatively determine the amount of NH_2 groups on the aminolysed PCL and biomolecule-immobilized PCL scaffolds. The experiment measured the absorbance at the wavelength of 538 nm using a UV-vis spectrophotometer. A calibration curve was obtained with known concentration of 1,6-hexamethylenediamine in 1,4-dioxane/IPA (1:1, v/v) solution as shown in Figure C1.

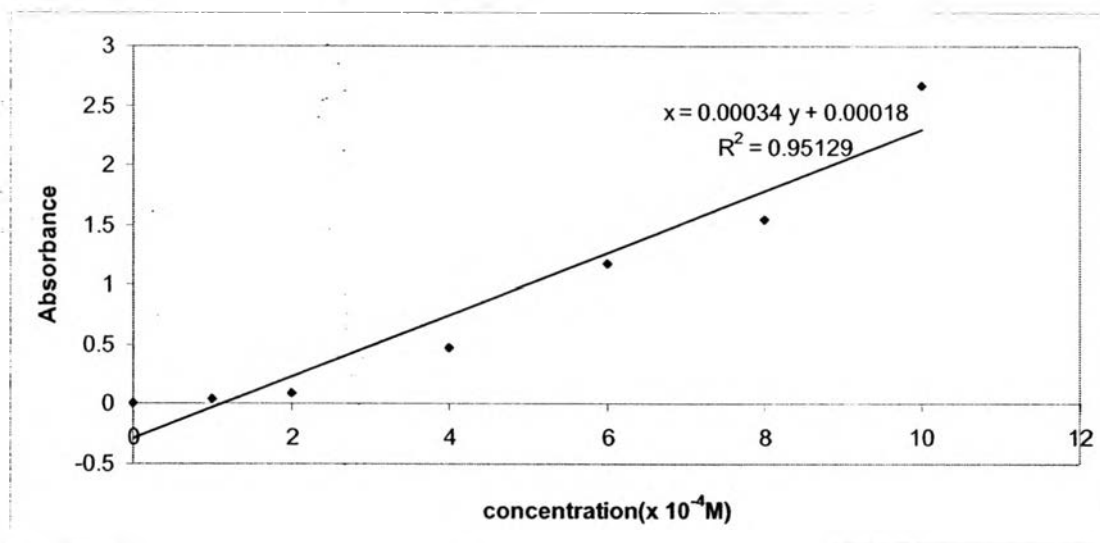


Figure C1 Calibration curve of UV absorbance as a function of 1,6-hexamethylenediamine (HMD) concentration analyzed by ninhydrin assay method

Table C1 NH₂ concentration and density as a function of 1,6-hexamethylenediamine

| 1,6-hexamethylenediamine concentration(g/ml) | Absorbance | NH ₂ concentration (x 10 ⁻⁴ M) | NH ₂ density (x10 ⁻⁷ mol/cm ²) |
|--|------------|--|--|
| 0.04 | 0.0085 | 1.84 | 1.20 |
| 0.06 | 0.012 | 1.87 | 1.21 |
| 0.08 | 0.02 | 1.88 | 1.22 |
| 0.1 | 0.0249 | 2.00 | 1.30 |
| 0.2 | 0.0598 | 2.10 | 1.37 |
| 0.4 | 0.0896 | 2.12 | 1.38 |

2. Elemental Composition of the Surface

The surface of neat and modified PCL fibrous scaffolds were further determined the elemental composition by using X-ray Photoelectron Spectrometer (XPS).

Table C2 Elemental compositions of C_{1s}, N_{1s}, O_{1s} and N_{1s}/C_{1s} ratio on the surface of aminolyzed PCL fibrous scaffolds as a function of 1,6-hexamethylenediamine

| Diamine concentration (g/ml) | C _{1s} | N _{1s} | O _{1s} | N _{1s} /C _{1s} ratio |
|------------------------------|-----------------|-----------------|-----------------|--|
| 0.04 | 76.52 | 0.48 | 23.01 | 0.0063 |
| 0.06 | 77.13 | 0.61 | 22.25 | 0.0079 |
| 0.08 | 75.93 | 1.24 | 22.84 | 0.0163 |
| 0.10 | 75.24 | 1.27 | 23.49 | 0.0169 |
| 0.20 | 76.3 | 1.3 | 22.4 | 0.0170 |
| 0.40 | 75.2 | 1.28 | 23.9 | 0.0170 |

Table C3 Elemental compositions of C_{1s} , N_{1s} , O_{1s} and N_{1s}/C_{1s} ratio on the surface of the neat, aminolyzed, and all types of immobilized PCL scaffolds

| Sample | C_{1s} | N_{1s} | O_{1s} | N_{1s}/C_{1s} ratio |
|--------------------------------|----------|----------|----------|--------------------------|
| Control PCL | 78.64 | 0.37 | 20.98 | 0.0047 |
| Aminolyzed PCL | 76.3 | 1.3 | 22.4 | 0.0170 |
| Activated PCL | 75.2 | 0.91 | 23.9 | 0.0121 |
| Gelatin type-A Immobilized PCL | 73.2 | 4.76 | 22.04 | 0.0650 |
| Gelatin type-B Immobilized PCL | 73.98 | 4.56 | 21.46 | 0.0616 |
| BSA Immobilized PCL | 73.4 | 3.5 | 23.1 | 0.0477 |
| CBP Immobilized PCL | 73.0 | 5.0 | 22.0 | 0.0685 |

APPENDICES

Appendix D Experimental Data of Cell Culture Studies

The potential use as bone scaffolds of PCL electrospun fibrous materials was evaluated using MC3T3-E1 cell culture studies, including direct cytotoxicity test, indirect cytotoxicity test, cell attachment, cell proliferation, ALP activity at 3 days and 7 days and mineralization as shown in Table D1, D2, D3, D4, D5, D6, and D7, respectively.

Table D1 Raw data of direct cytotoxicity test of proteins, which were immobilized onto the PCL fibrous scaffolds, determined the viability of cells by MTT assay method at 570 nm

| Time(day) | % viability of MC3T3-E1 cells (relative to 2%MEM at 1 day) | | | | | |
|----------------|--|------|--------|------|--------|-------|
| | 1 | | 2 | | 3 | |
| Material | avg | SD | avg | SD | avg | SD |
| 2%MEM(control) | 100.00 | 0.22 | 140.15 | 8.77 | 182.45 | 0.35 |
| gelatin | 95.78 | 4.06 | 110.17 | 5.57 | 169.02 | 7.43 |
| gelatin | 103.02 | 5.34 | 134.65 | 8.26 | 168.01 | 6.62 |
| BSA | 100.64 | 2.73 | 137.67 | 8.32 | 172.41 | 14.78 |
| CBP | 83.50 | 3.82 | 128.14 | 5.27 | 148.90 | 8.75 |

Table D2 Raw data of indirect cytotoxicity test of all types of PCL fibrous scaffolds, determined the viability of cells by MTT assay method at 570 nm

| Time(day) | % viability of MC3T3-E1 cells (relative to TCPs at 1 day) | | | | | |
|--------------------------|---|------|--------|-------|--------|-------|
| | 1 | | 2 | | 3 | |
| Material | avg | SD | avg | SD | avg | SD |
| TCPs (control) | 100.00 | 0.22 | 140.15 | 8.77 | 182.45 | 0.35 |
| neat PCL | 94.78 | 4.57 | 109.62 | 1.16 | 150.14 | 0.24 |
| aminolysed PCL | 100.00 | 2.00 | 113.29 | 1.81 | 157.42 | 4.48 |
| activated PCL | 104.86 | 4.56 | 121.54 | 5.16 | 159.49 | 10.11 |
| gelatinA immobilized PCL | 103.57 | 0.89 | 119.71 | 1.81 | 152.06 | 1.19 |
| gelatinB immobilized PCL | 104.40 | 2.76 | 129.42 | 8.96 | 156.32 | 7.98 |
| BSA immobilized PCL | 102.57 | 2.26 | 143.08 | 11.55 | 157.84 | 1.19 |
| CBP immobilized PCL | | | | | | |

Table D3 Raw data of cell attachment of MC3T3-E1 onto all types of PCL fibrous scaffolds at 2, 4, and 6 hours, determined the viability of cells by MTT assay method at 570 nm

| Time(h) | % viability of MC3T3-E1 cells (relative to TCPs at 2 h) | | | | | |
|--------------------------|---|-------|--------|-------|--------|-------|
| | 2 | | 4 | | 6 | |
| Material | avg | SD | avg | SD | avg | SD |
| TCPs | 100.00 | 18.03 | 170.08 | 23.37 | 256.97 | 39.81 |
| neat PCL | 154.92 | 24.16 | 154.10 | 25.48 | 136.48 | 17.41 |
| aminolysed PCL | 113.93 | 19.33 | 110.66 | 33.28 | 131.56 | 17.26 |
| activated PCL | 112.70 | 43.59 | 103.69 | 13.23 | 137.70 | 42.09 |
| gelatinA immobilized PCL | 101.23 | 12.92 | 108.20 | 21.30 | 131.56 | 18.39 |
| gelatinB immobilized PCL | 118.44 | 47.12 | 108.20 | 18.02 | 131.56 | 20.73 |
| BSA immobilized PCL | 118.03 | 23.89 | 118.85 | 18.40 | 143.44 | 34.27 |
| CBP immobilized PCL | 143.59 | 18.48 | 147.44 | 22.00 | 175.64 | 22.28 |

Table D4 Raw data of cell proliferation of MC3T3-E1 onto all types of PCL fibrous scaffolds at 1, 2, and 3 days, determined the viability of cells by MTT assay method at 570 nm

| time(day) | % viability of MC3T3-E1 cells (relative to TCPs at 1 day) | | | | | |
|--------------------------|---|-------|--------|-------|--------|--------|
| | 1 | | 2 | | 3 | |
| Material | avg | SD | avg | SD | avg | SD |
| TCPs (control) | 100.00 | 8.83 | 126.80 | 13.27 | 132.91 | 8.82 |
| neat PCL | 117.05 | 7.33 | 240.03 | 61.14 | 292.20 | 52.33 |
| aminolysed PCL | 116.95 | 55.56 | 321.13 | 79.59 | 450.10 | 85.67 |
| activated PCL | 106.70 | 12.84 | 426.90 | 71.86 | 471.00 | 76.92 |
| gelatinA immobilized PCL | 80.97 | 12.68 | 332.06 | 84.07 | 805.36 | 59.13 |
| gelatinB immobilized PCL | 78.34 | 11.32 | 392.32 | 62.06 | 804.94 | 183.19 |
| BSA immobilized PCL | 144.90 | 10.42 | 498.09 | 43.30 | 840.39 | 62.77 |
| CBP immobilized PCL | 221.08 | 7.38 | 450.98 | 17.53 | 789.22 | 57.29 |

Table D5 Raw data of ALP Activity of MC3T3-E1 seeded onto all types of PCL fibrous scaffolds at 3 days

| Time(h) | ALP activity test (3 days) | | | | | | | |
|--------------------------|----------------------------|---------------|--------------|-----------|---------------|--------------|--------------|------|
| | 1 | | | 2 | | | ALP activity | |
| Material | ALP assay | protein assay | ALP activity | ALP assay | protein assay | ALP activity | avg | SD |
| TCPs | 2.73550 | 13.97004 | 0.19581 | 2.33871 | 9.03533 | 0.26 | 0.23 | 0.04 |
| Neat PCL | 6.81594 | 28.72645 | 0.23727 | 6.07297 | 40.78989 | 0.15 | 0.19 | 0.06 |
| Aminolysed PCL | 5.42109 | 26.95169 | 0.20114 | 5.67283 | 48.05050 | 0.12 | 0.16 | 0.06 |
| Activated PCL | 5.52195 | 34.51732 | 0.15998 | 7.30696 | 50.52417 | 0.14 | 0.15 | 0.01 |
| GelatinA immobilized PCL | 5.97322 | 27.07740 | 0.22060 | 6.81594 | 34.78842 | 0.20 | 0.21 | 0.02 |
| GelatinB immobilized PCL | 7.06182 | 28.47695 | 0.24798 | 7.11091 | 36.98263 | 0.19 | 0.22 | 0.04 |
| BSA immobilized PCL | 3.76878 | 21.10507 | 0.17857 | 7.79525 | 19.12051 | 0.41 | 0.29 | 0.16 |
| CBP immobilized PCL | 11.54670 | 54.51166 | 0.21182 | 10.99686 | 56.78298 | 0.19 | 0.20 | 0.01 |

Table D6 Raw data of ALP Activity of MC3T3-E1 seeded onto all types of PCL fibrous scaffolds at 7 days

| Time(h) | ALP activity test (3 days) | | | | | | | |
|--------------------------|----------------------------|---------------|--------------|-----------|---------------|--------------|--------------|------|
| | 1 | | | 2 | | | ALP activity | |
| Material | ALP assay | protein assay | ALP activity | ALP assay | protein assay | ALP activity | avg | SD |
| TCPs | 4.137722 | 1.987754 | 2.08 | 3.340162 | 1.29369 | 2.58 | 2.33 | 0.35 |
| Neat PCL | 4.398301 | 2.164105 | 2.03 | 4.810824 | 3.333577 | 1.44 | 1.74 | 0.42 |
| Aminolysed PCL | 9.826533 | 5.966295 | 1.65 | 6.222275 | 4.632124 | 1.34 | 1.50 | 0.21 |
| Activated PCL | 8.765606 | 2.969726 | 2.95 | 9.200245 | 5.199743 | 1.77 | 2.36 | 0.84 |
| GelatinA immobilized PCL | 5.622587 | 4.257312 | 1.32 | 6.668014 | 4.915135 | 1.36 | 1.34 | 0.03 |
| GelatinB immobilized PCL | 9.682136 | 4.915135 | 1.97 | 7.6977883 | 4.538146 | 1.70 | 1.83 | 0.19 |
| BSA immobilized PCL | 10.83588 | 4.915135 | 2.20 | 10.06705 | 3.333577 | 3.02 | 2.61 | 0.58 |
| CBP immobilized PCL | 109.53133 | 56.87312085 | 1.93 | 104.31555 | 59.24283422 | 1.76 | 1.84 | 0.12 |

Table D7 Raw data of quantity of mineral deposition on all types of PCL fibrous scaffolds using Alizarin Red-S method at 570 nm

| Materials | 1 | 2 | avg | SD |
|--------------------------------|----------|----------|------------|-----------|
| TCPS | 0.025 | 0.03 | 0.0275 | 0.003536 |
| Neat PCL | 0.393 | 0.401 | 0.397 | 0.005657 |
| Aminolyzed PCL | 0.394 | 0.392 | 0.393 | 0.001414 |
| Activated PCL | 1.347 | 1.179 | 1.263 | 0.118794 |
| Gelatin type-A immobilized PCL | 1.841 | 1.886 | 1.8635 | 0.03182 |
| Gelatin type-B immobilized PCL | 1.839 | 1.389 | 1.614 | 0.318198 |
| BSA immobilized PCL | 1.44 | 1.864 | 1.652 | 0.299813 |
| CBP immobilized PCL | 3.61 | 2.517 | 3.0635 | 0.772868 |

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Presentations:

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