## การเตรียมและประเมินอนุภาคขนาดเล็กที่ย่อยสลายได้ทางชีวภาพของไรแฟมพิชิน โดยใช้เทคนิคสารไหลที่สภาวะเหนือจุดวิกฤตเพื่อนำส่งยาทางปอด



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วิทยานิพนธ์นี้เป็นส่วนหนึ่งของการศึกษาตามหลักสูตรปริญญาเภสัชศาสตรดุษฎีบัณฑิต สาขาวิชาเภสัชกรรม คณะเภสัชศาสตร์ จุฬาลงกรณ์มหาวิทยาลัย ปีการศึกษา 2548 ISBN 974-17-4558-3 ลิขสิทธิ์ของจุฬาลงกรณ์มหาวิทยาลัย

# PREPARATION AND EVALUATION OF BIODEGRADABLE RIFAMPICIN MICROPARTICLES USING SUPERCRITICAL FLUID TECHNIQUE FOR PULMONARY DELIVERY

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วิภาลักษณ์ ปฐมชัยวิวัฒน์: การเตรียมและประเมินอนุภาคขนาดเล็กที่ย่อยสลายได้ทางชีวภาพของ ไรแฟมพิชินโดยใช้เทคนิคสารไหลที่สภาวะเหนือจุดวิกฤตเพื่อนำส่งยาทางปอด (PREPARATION AND EVALUATION OF BIODEGRADABLE RIFAMPICIN MICROPARTICLES USING SUPERCRITICAL FLUID TECHNIQUE FOR PULMONARY DELIVERY) อ. ที่ปรึกษา: รศ.ดร. พจน์ กูลวานิช, อ. ที่ปรึกษาร่วม: ผศ.ดร. อรลักษณา แพรัตกูล, 187 หน้า. ISBN 974-17-4558-3

งานวิจัยนี้ใช้เทคนิคสารใหลที่สภาวะเหนือจุดวิกฤต เพื่อเตรียมอนุภาคขนาดเล็กของไรแฟมพิซินและพอลิ เมอร์ที่สามารถย่อยสลายได้ทางชีวภาพเพื่อสูดคมเข้าสู่ปอดได้ พอลิเมอร์ที่ใช้ทคลองเป็นกลุ่มของโพลีไฮครอกซีแอซิด พอลิเมอร์ ได้แก่ 50:50 พอลิ(ดีแอล-แลคไทด์-โค-ไกลโคไลด์)(PLGA) พอลิ(ดีแอล-แลคไทด์)( DL-PLA) และ พอลิ ละลายไรแฟมพิซินและพอลิเมอร์ที่อัตราส่วนต่างๆในเมทิลีนคลอไรค์แล้วสเปรย์ลงใน (แอล-แลคไทด์)(L-PLA) คาร์บอนไดออกใชด์ที่อยู่ในสภาวะเหนือจุดวิกฤต สึกษาถึงผลของชนิดและปริมาณพอลิเมอร์ ความดัน อุณหภูมิ ความ เข้มข้นของสารละลาย อัตราการป้อนสาร ต่อลักษณะของผลิตภัณฑ์ที่ได้ เมื่อใช้พอลิ(ดีแอล-แลคไทค์-โค-ไกลโคไลค์) และพอลิ(คีแอล-แลคไทค์)ระหว่าง 50 ถึง 100% จะได้ฟิล์มของพอลิเมอร์หรือฟิล์มของพอลิเมอร์กับตัวยา เมื่อใช้พอลิ (คีแอล-แลคไทค์-โค-ไกลโคไลค์)และพอลิ(ดีแอล-แลคไทค์)ระหว่าง 20 ถึง 40% จะได้อนุภาคที่มีขนาคใหญ่กว่า 18 ไมครอนและเมื่อใช้พอลิ(แอล-แลคไทค์)ระหว่าง 70 ถึง 100% จะได้อนุภาคทรงกลมขนาดเล็ก เมื่อใช้พอลิ(แอล-แลค ไทค์)ที่ 60% จะได้ทั้งอนุภาคทรงกลมขนาดเล็กและอนุภาคที่มีรูปร่างไม่แน่นอน เมื่อลดปริมาณของพอลิ(แอล-แลค ไทค์)ลงอีกจะพบเพียงอนุภาคที่มีรูปร่างไม่แน่นอน อนุภาคขนาคเล็กที่ผลิตโคยใช้ปริมาณของพอลิ(แอล-แลคไทค์) 60% และไรแฟมพิซิน 40% กักเก็บยาได้ดี (23.30%) และมีขนาดอนุภาคเฉลี่ยโดยปริมาตรเท่ากับ 4.07 ไมครอน แต่ ปลดปล่อยยาค่อนข้างรวดเร็ว อนุภาคขนาดเล็กที่ผลิตโดยใช้ปริมาณของพอลิ(แอล-แลคไทด์) 70% และไรแฟมพิชิน 30% เป็นสูตรตำรับที่เหมาะสมเนื่องจากสามารถกักเก็บยาได้ดี (16.33%) มีขนาดอนุภาคเฉลี่ยโดยปริมาตรเท่ากับ 3.40 ใมครอน และสามารถปลดปล่อยยาอย่างต่อเนื่องได้ตลอด 24 ชั่วโมง อนภาคขนาดเล็กที่ผลิตโดยใช้ปริมาณของพอลิ (แอละแลคไทค์) 80% และไรแฟมพิซิน 20% กักเก็บยาต่ำ (8.13%) มีขนาคอนุภาคเฉลี่ยโดยปริมาตรเท่ากับ 3.37 ไมครอน และปลดปล่อยยาค่อนข้างช้า ขนาคอนุภาคเฉลี่ยแบบแอโรไคแนมิก (mass median aerodynamic diameter) ของสูตรตำรับที่เตรียมได้จากพอลิ(แอล-แลคไทด์) 70% และไรแฟมพิซิน 30% กับแลคโตสขนาดเล็กกว่า 45 ไมครอน ในอัตราส่วน 1:2 เท่ากับ 4.86 ใมครอน และเมื่อผสมกับแลคโตสขนาคระหว่าง 45 ถึง 90 ใมครอนในอัตราส่วน 1:2 เท่ากับ 4.29 ใมครอน อนุภาคของพอถิ(แอล-แลคไทค์)กับเก็บไรแฟมพิซินที่เครียมจากกระบวนการคึงตัวทำละลายที่ ใช้สภาวะสารใหลเหนือจุดวิกฤต (supercritical antisolvent process) เหมาะสมสำหรับใช้เครียมผลิตภัณฑ์ยาสูดคมแบบ ผงแห้งเพื่อนำส่งยาทางปอคเนื่องจากมีขนาคของอนภาคที่เหมาะสม ไม่พบว่ามีการสถายของไรแฟมพิซินเมื่อเครียมตัว ยาด้วยกระบวนการที่ใช้สภาวะสารใหลเหนือจุดวิกฤต การวิเคราะห์โดยใช้ XRD, FTIR และDSC แสดงว่าไรแฟมพิชิน ที่ผ่านกระบวนการดังกล่าวได้สารที่มีรูปผลึกไม่เหมือนกับรูปผลึกที่มีการรายงานก่อนหน้านี้ น้ำหนักโมเลกุลและแหล่ง ผลิตพอลิเมอร์มีอิทธิพลต่อคุณสมบัติของอนุภาคขนาดเล็กที่ได้ ประสิทธิภาพในการต่อค้านการเจริญเติบโตของเชื้อไม โครแบคทีเรียทูเบอร์คูโลซีสของอนุภาคพอลิ(แอล-แลคไทค์)กักเก็บไรแฟมพิชินที่เตรียมจากกระบวนการที่ใช้สภาวะ สารไหลเหนือจุดวิกฤตยังเท่าเทียมกับตัวยาไรแฟมพิชินก่อนผ่านกระบวนการ

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It is of interest to apply a supercritical fluid technology for production of inhalable biodegradable microparticles of rifampicin. The polyhydroxy acids[poly(DLlactide-co-glycolide) copolymer composition 50:50 (PLGA), poly(DL-lactide)(DL-PLA), and poly(L-lactide)(L-PLA)] were used for preparation of drug-loaded microparticles. The solutions of rifampicin and polymer in methylene chloride at various ratios were sprayed into supercritical carbon dioxide. The effect of the type and content of polymer, operating pressure, temperature, solution concentration and feed rate of solution on the characteristics of products were investigated. With 50-100% polymer content of DL-PLA and PLGA, polymer or polymer-drug film occurred. The DL-PLA and PLGA microparticles of 20-40% polymer content had volumetric mean diameter larger than 18 µm and exhibited irregular shape particles forming large and porous agglomerates. The spherical drug loaded microparticles of L-PLA polymer was formed at high polymer content (70-100%). The microparticles prepared using 60% L-PLA polymer content was in spherical and irregular shapes. The shape of L-PLA microparticles became more irregular with decreasing polymer content. The microparticles prepared from 60 % L-PLA and 40 % rifampicin had good drug loading (23.30%) and a mean size of 4.07 µm but their release of drug was rather rapid. The microparticles prepared from 70 % L-PLA and 30 % rifampicin was the preferred formula because it had good drug loading (16.33%) with mean of 3.40 µm and showed sustained release property throughout 24 hours. The microparticles prepared from 80% L-PLA and 20% rifampicin had low drug loading (8.13%) with mean size of 3.37 µm and their releases of drug was rather slow. The mass medium aerodynamic diameter of the microparticles prepared from 70 % L-PLA and 30 % rifampicin with lactose (< 45 um) in 1:2 ratio and with lactose (45-90 μm) in 1:2 ratio were 4.86 μm and 4.29 μm, respectively. L-PLA rifampicin loaded microparticles prepared by supercritical anti-solvent (SAS) process was of a suitable size to be used in dry powder inhaler formulation for pulmonary delivery. SAS process showed that no decomposition of rifampicin occurred during the processing. The analysis from XRD, FTIR and DSC indicated that processed rifampicin produced by SAS technique was not corresponding to that of rifampicin in the previous reports. Not only the molecular weight of polymer but also the source of polymer influenced on the characteristics of microparticles. The bactericidal efficacy of L-PLA rifampicin loaded microparticles produced by SAS technique against Mycobacterium Tuberculosis was similar to that of unprocessed rifampicin.

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#### **ABBREVIATIONS**

bar 10<sup>5</sup> Pa (one newton per square meter)

°C degree Celsius

cm centimeter

cm<sup>2</sup> square centimeter

CV coefficient of variation

 $D_{10\%}$  particle diameters at a cumulative fraction of the volume distribution at

10 percent (μm)

D<sub>50%</sub> particle diameters at a cumulative fraction of the volume distribution at

50 percent (μm)

D<sub>90%</sub> particle diameters at a cumulative fraction of the volume distribution at

90 percent (μm)

DL-PLA poly(DL-lactide)

DL-PLGA poly(DL-lactide-co-glycolide) copolymer

e.g. exemplit gratia, 'for example'

et al. et alii, 'and others'

g gram

HPLC high performance liquid chromatography

hr hour

Kg kilogram

L-PLA L-poly(lactide)

mg milligram

min minute
ml milliliter

mm millimeter

MPa Megapascals

nm nanometer

MW molecular weight

N normal (concentration)

N/m<sup>2</sup> Newton per square meter

N-s/m<sup>2</sup> Newton-second per square meter

Pa pascal

PBS phosphate buffer in saline

pH the negative logarithm of the hydrogen ion concentration

ppm part per million

psi pound per square inch

r<sup>2</sup> coefficient of determination

rpm revolution per minute

SAS supercritical anti-solvent

SD standard deviation

sec second

SEM Scanning Electron Microscope

SF Supercritical Fluid

Span The polydispersity of the microparticles was  $[D_{90\%}-D_{10\%}]/D_{50\%}$ 

T<sub>g</sub> glass transition temperature

T<sub>m</sub> melting temperature

μl microliter

μg microgram

μm micrometer

USP The United States Pharmacopoeia

Vs versus

%w/w % weight by weight

%w/v % weight by volume